

ESTIMATION OF FEMORAL FE STRENGTH FOR THE FRACTURE PREDICTION IN RETROSPECTIVE AND PROSPECTIVE STUDIES

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Introduction

Finite element (*FE*) models (*FEM*) from CT data are promising to assess bone strength (*FEBS*) and the risk of fracture in-vivo. They have demonstrated a high accuracy in predicting bone strains and bone strength in-vitro. However, when tested on clinical cases [Amin, 2011; Keyak, 2011; Orwoll, 2009] they did not show a clear superiority over areal bone mineral density (aBMD). The aim of this work is to explore the clinical predictivity of *FEBS* derived from a validated subject-specific *FEM* procedure [Schileo, 2008] in a case-control retrospective study (*RS*) and in a nested case-control prospective study (*PS*).

Methods

Retrospective Study: 22 incident low trauma proximal femur fractures (*F*) and 33 controls (*NF*) were enrolled at Istituto Ortopedico Rizzoli. All patients were osteopenic or osteoporotic and received a full femoral CT (in acute conditions for fractured cases) and a DXA exam.

Prospective study: 21 women on which proximal femur fractures (*F*) were prospectively observed, and 45 sex and age-matched controls (*NF*) were selected from the AGES-Reykjavik Study. For each individual, baseline proximal femur CT scans and simulated DXA aBMD values from QCT were available.

The *FE* models were generated from CT [Schileo, 2008]. *FEBS*, evaluated in a number of quasi-axial configurations to mimic the in-vivo variability of hip reactions, was defined as the minimum load inducing on the femoral neck surface an $\epsilon > \epsilon_{lim}$ [Bayraktar, 2004].

We tested the ability of *FEBS* and aBMD to: 1) discriminate between fracture cases and controls; 2) individually classify cases at risk.

Results and Discussion

In both studies, *FEBS* had a limited correlation with aBMD (Spearman $r \sim 0.5$ vs ~ 0.8 reported in [Orwoll, 2009; Amin, 2011]). *FEBS* and aBMD showed a lower mean value in *F* group compared to the *NF* group in both studies. The mean differences were: 1) notably higher for *FEBS* in the *RS* (33%, $p < 0.0001$, vs 12% for aBMD, $p = 0.01$); 2) slightly higher for *FEBS* in the *PS* (19%, p -value < 0.0003 , vs 15% for aBMD, p -value < 0.004). The mean *FEBS* differences were higher than [Keyak, 2011].

To test the ability of *FEBS* and aBMD to individually classify cases, logistic regressions and ROC curves were derived for *FEBS* and aBMD obtaining: 1) in the *RS*, a superiority of *FEBS* vs aBMD in classifying *F* and *NF* (AUC=0.88 vs 0.71, higher than [Amin, 2011]) and 2) in the *PS*, a slightly better performance for *FEBS* than aBMD (AUC=0.78 vs. 0.72), though the maximum classification ability reached so far in this study (AUC=0.80, combining *FEBS* and aBMD in the regression) does not improve over the existing literature. However, when including both *FEBS* and aBMD in the regression, in both studies only *FEBS* was retained as statistically significant. These results confirm the potential of the proposed *FE* method to clinically identify fractured cases, despite two limitations: 1) in the *PS*, the change of bone material properties with time was not modelled (future work); 2) in both *RS* and *PS*, falls to the side were not modelled (ongoing).

References

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